

Historical development of CR/DR and new detector technologies

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Learning Objectives

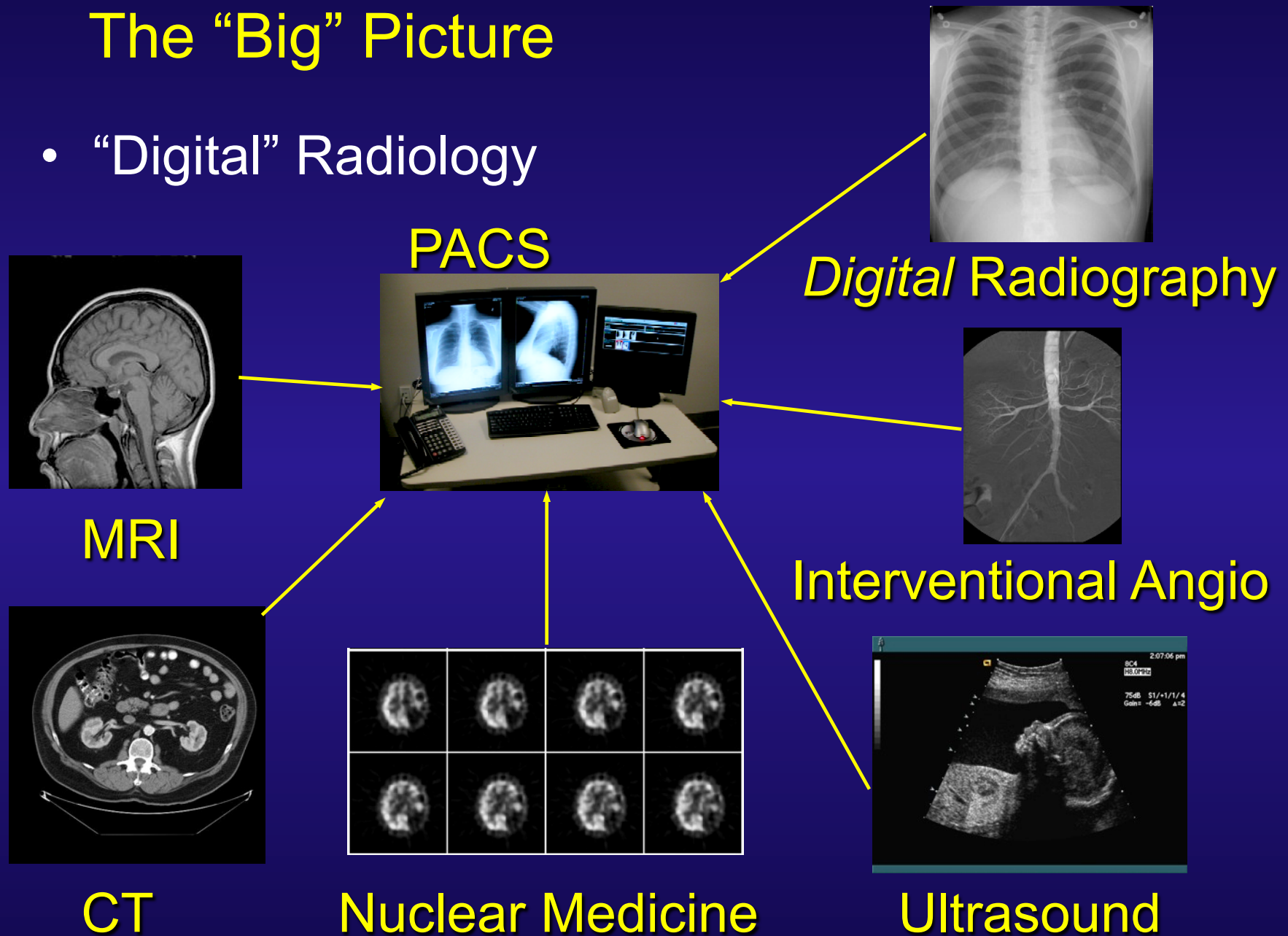
- Explain technology of available and future digital radiography technology
- Understand underlying system operation and characteristics
- Compare CR – DR - Novel image acquisition advantages and disadvantages

DIGITAL IMAGING IN RADIOLOGY

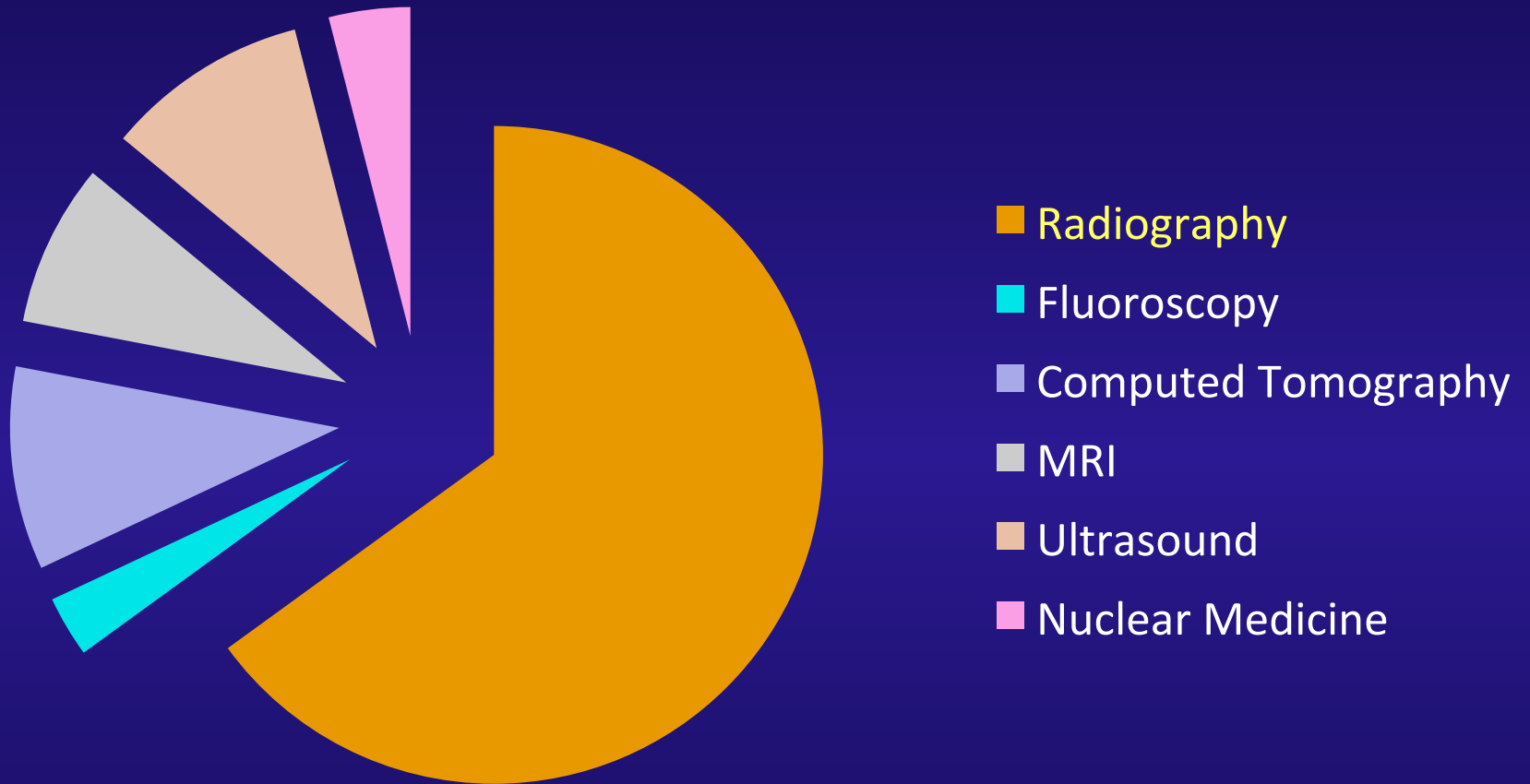
- *Digital* imaging is an *essential* component of Electronic Imaging, Telemedicine and Remote Diagnosis
- Steps for digital imaging
 - Acquisition
 - Display
 - Diagnosis
 - Distribution
 - Archive

The “Big” Picture

- “Digital” Radiology



Imaging Volume



Projection imaging: 60% - 70% of medical imaging

But First..... CR & DR

- An intrinsic part of the PACS
- Historically, the last electronically integrated
- Lots of changes in the past decade.....

Digital x-ray detector

1. Acquisition

Transmitted x-rays
through patient

Digital Pixel
Matrix

Charge
collection
device

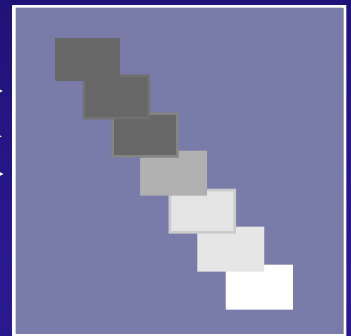
X-ray converter
x-rays \rightarrow electrons

Analog to Digital
Conversion

Digital
processing

2. Display

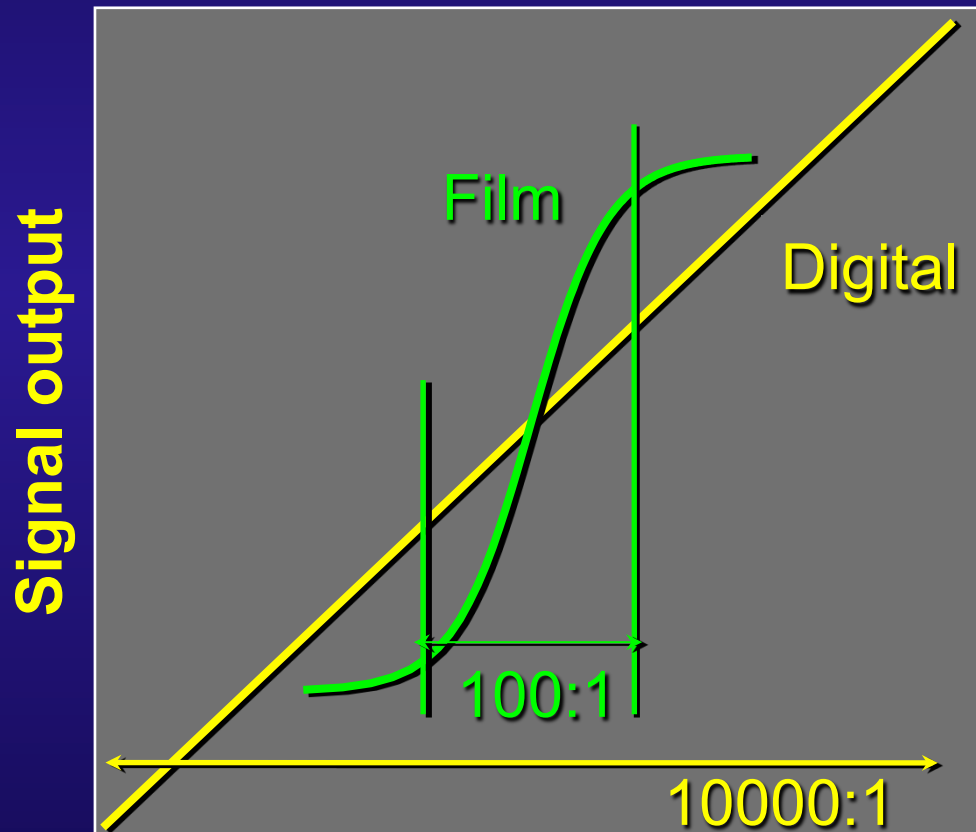
Digital to Analog
Conversion



3. Archiving

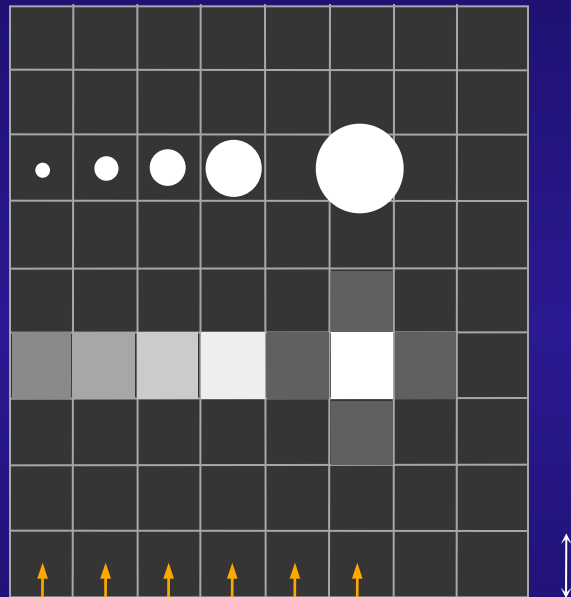
Analog versus Digital

Exposure Latitude



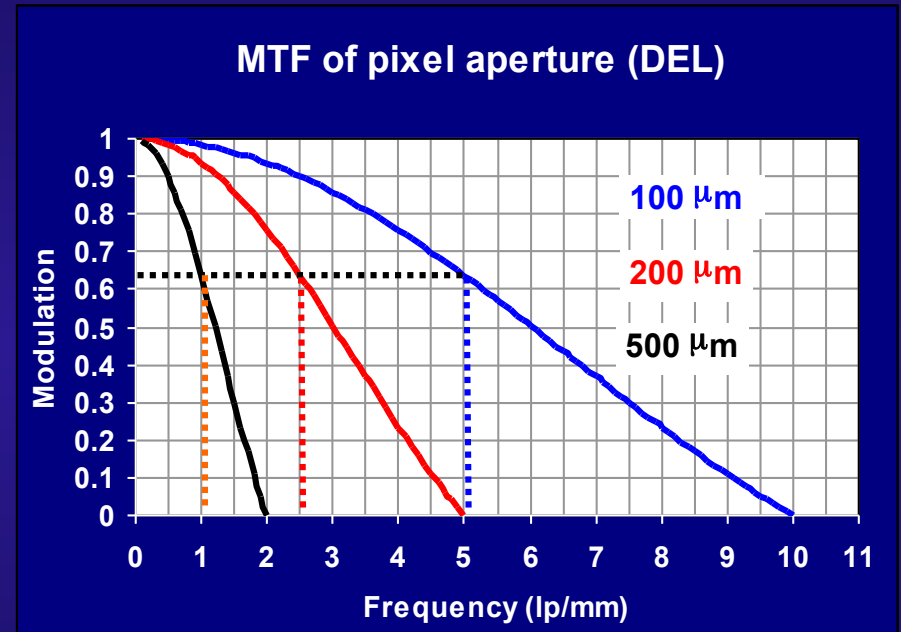
Digital sampling

Spatial Resolution



Sampling
Pitch

Detector
Element,
"DEL"



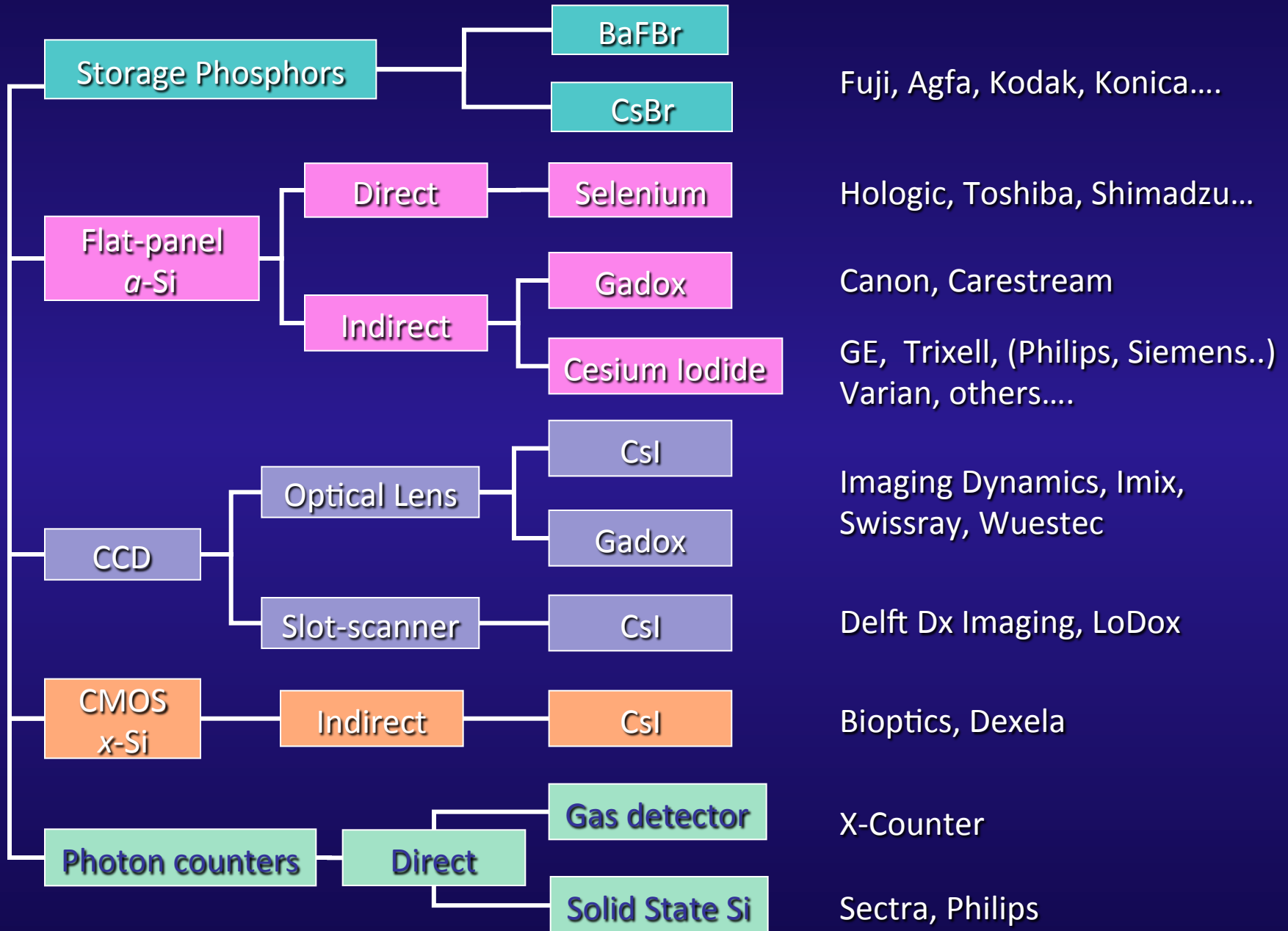
Fourier transform of Rect (Dx) = sinc(Dx)

Cutoff frequency $f_c = (Dx)^{-1}$

With sampling pitch = sampling aperture, Dx

Nyquist Frequency $f_N = (2 Dx)^{-1}$

Digital Radiography 2013: detectors and manufacturers



Digital Radiography common themes

- Separation of Acquisition, Display, and Archive
- Wide dynamic range
 - ~ 0.01 to 100 mR (~ 0.1 to 1000 mGy) incident exposure
- Variable detector exposure operation
 - 20 to 2000 “speed class”
- Appropriate SNR & image processing are *crucial* for image optimization

Categorization of digital radiography detectors

- Detector form factor
 - Cassette versus cassette-less



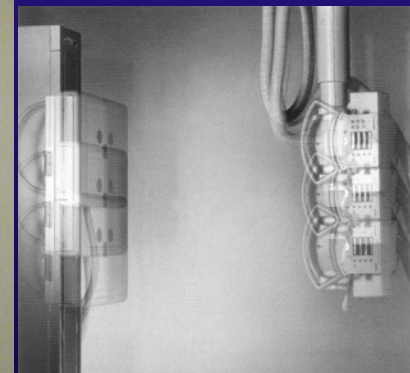
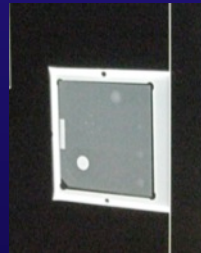
PSP
cassette

Line-scan PSP
detector system



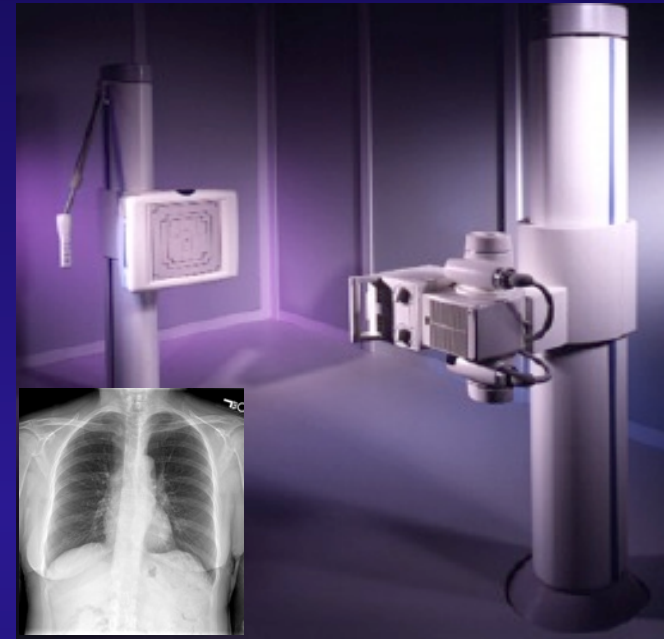
Slot-scan CXR system

- Passive versus active x-ray detection



Categorization of digital radiography detectors

- Image acquisition geometry
 - Large FOV (milliseconds)
 - Reduced patient motion
 - Real-time operation possibilities
 - Anti-scatter grid necessary
 - Slot-scan (seconds)
 - Reduced scatter
 - Lower patient dose
 - Possible motion problems



Available digital radiography technology 2013

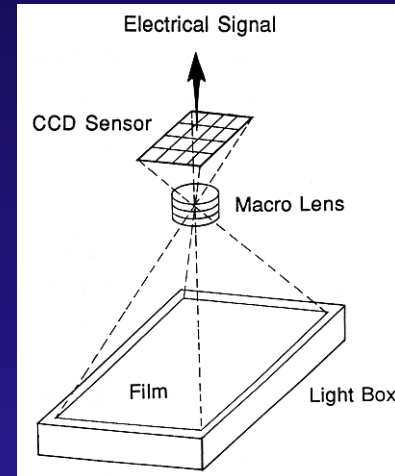
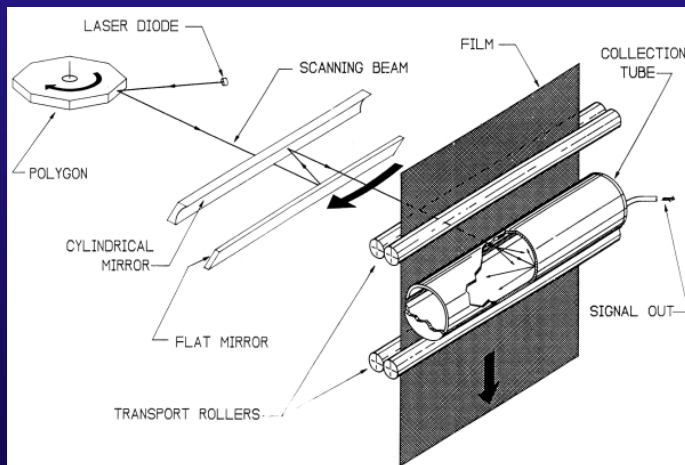
- CR: Photostimulable Storage Phosphor (PSP)
 - Cassette-based detectors/readers
 - Flying spot mechanical changers
 - Line scan integrated detectors
- CCD: Charge-Coupled Device
 - 2-D lens coupled systems
 - 1-D slot-scan systems
- Thin-Film-Transistor (TFT) flat panel
 - Indirect detection (scintillator)
 - Direct detection (semi-conductor)
 - Portable wireless implementations
- Photon Counting slot-scan systems

“In-progress” technologies

- X-ray energy sensitive counters: gas or silicon strip detectors
- Complementary Metal Oxide Semiconductor (CMOS)
- Hybrid direct / indirect flat panel TFT with variable gain
- X-ray “light valve” Liquid Crystal / scanner detector system

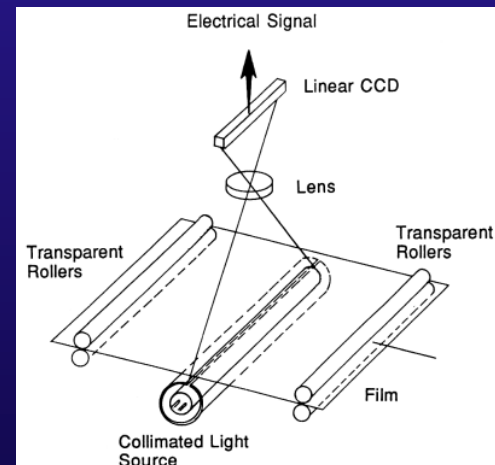
Starting point: Analog film digitization

- Video of trans-illuminated radiographs
 - “Camera on a stick”
 - Low cost, low quality
- Film digitizers
 - LASER
 - Better quality
 - Not reliable



CCD Array

Limited dynamic range
Very reliable



Computed Radiography (CR)

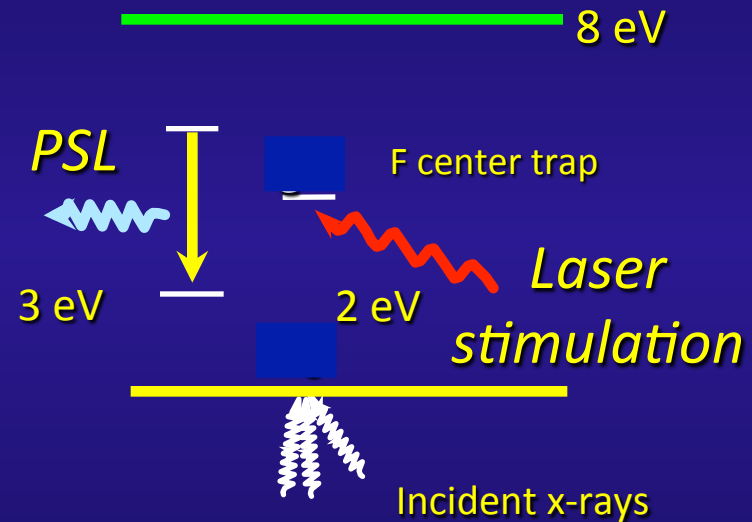
- *The* first clinically useful technology available for large field-of-view digital imaging
- Based upon the principles of photostimulated luminescence; 30+ years of experience
- Operation emulates the screen-film paradigm in use and handling.. (flexible, but labor intensive)
- Manufacturing trends:
 - Smaller, faster, less expensive

PSP Detector

- Photostimulable Storage Phosphor (PSP)

Phosphor Plate

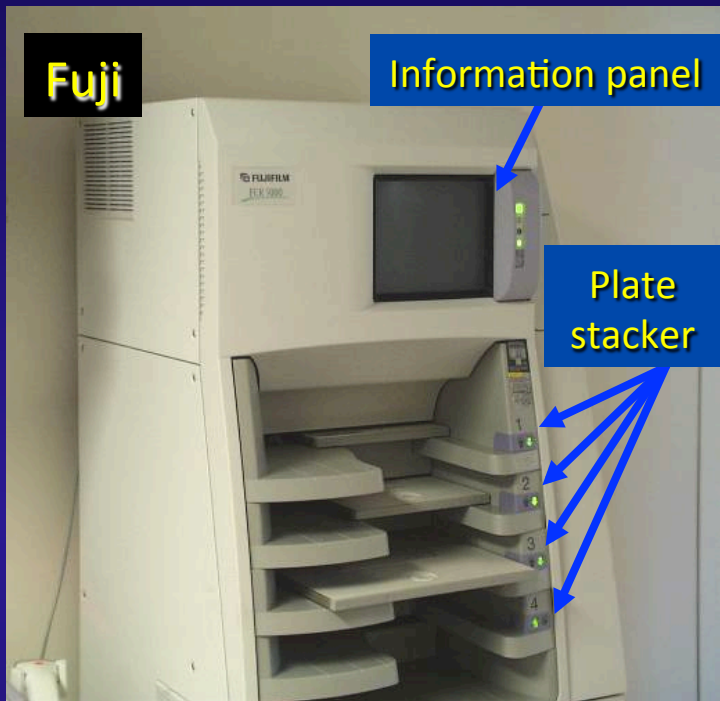
Cassette Holder



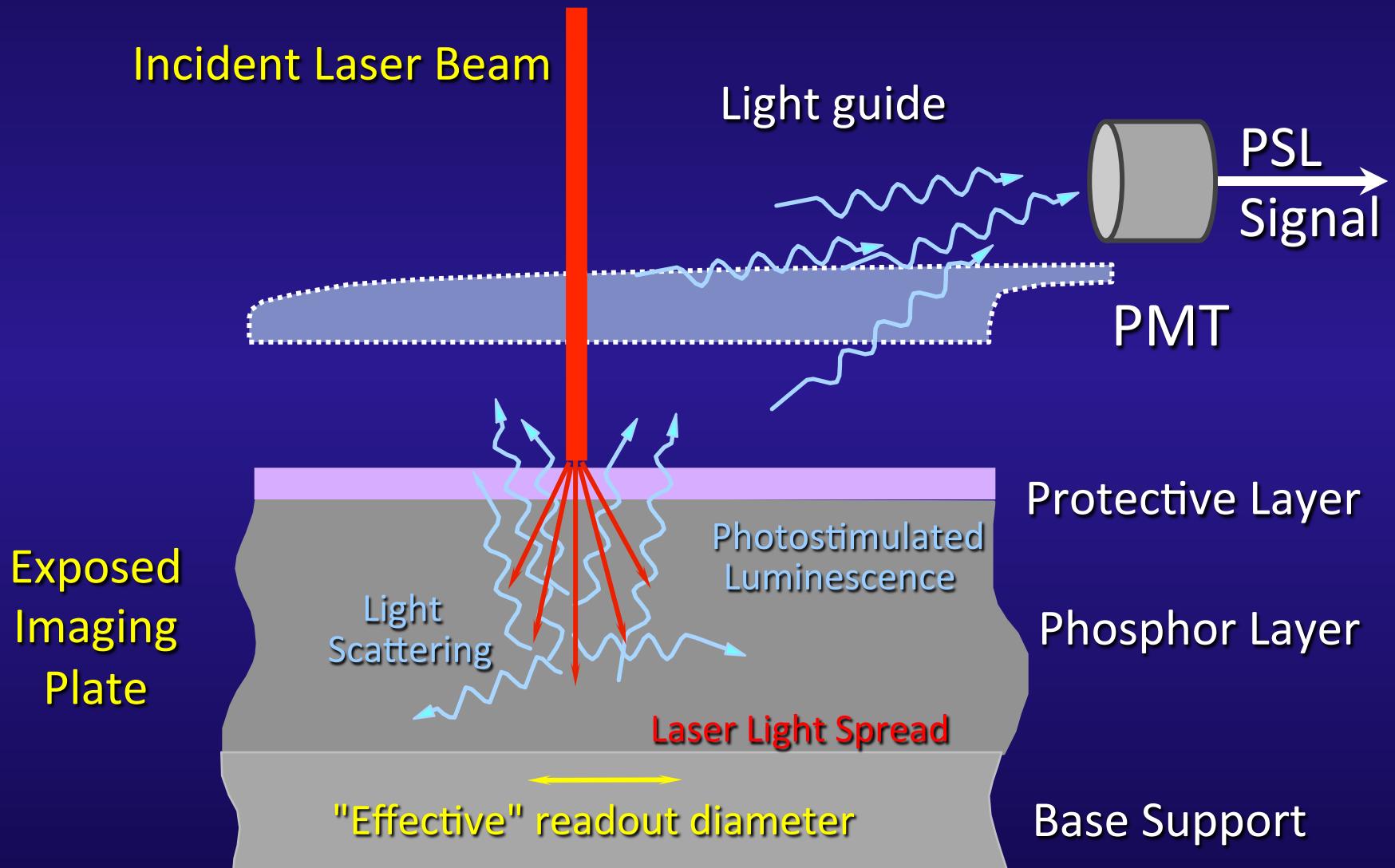
- Coating thickness:
 - Standard resolution: ~100 mm BaFBr
 - High resolution: ~50-70 mm BaFBr
- Enhancements: Dual-side read; structured phosphor – CsBr

Computed Radiography “reader”

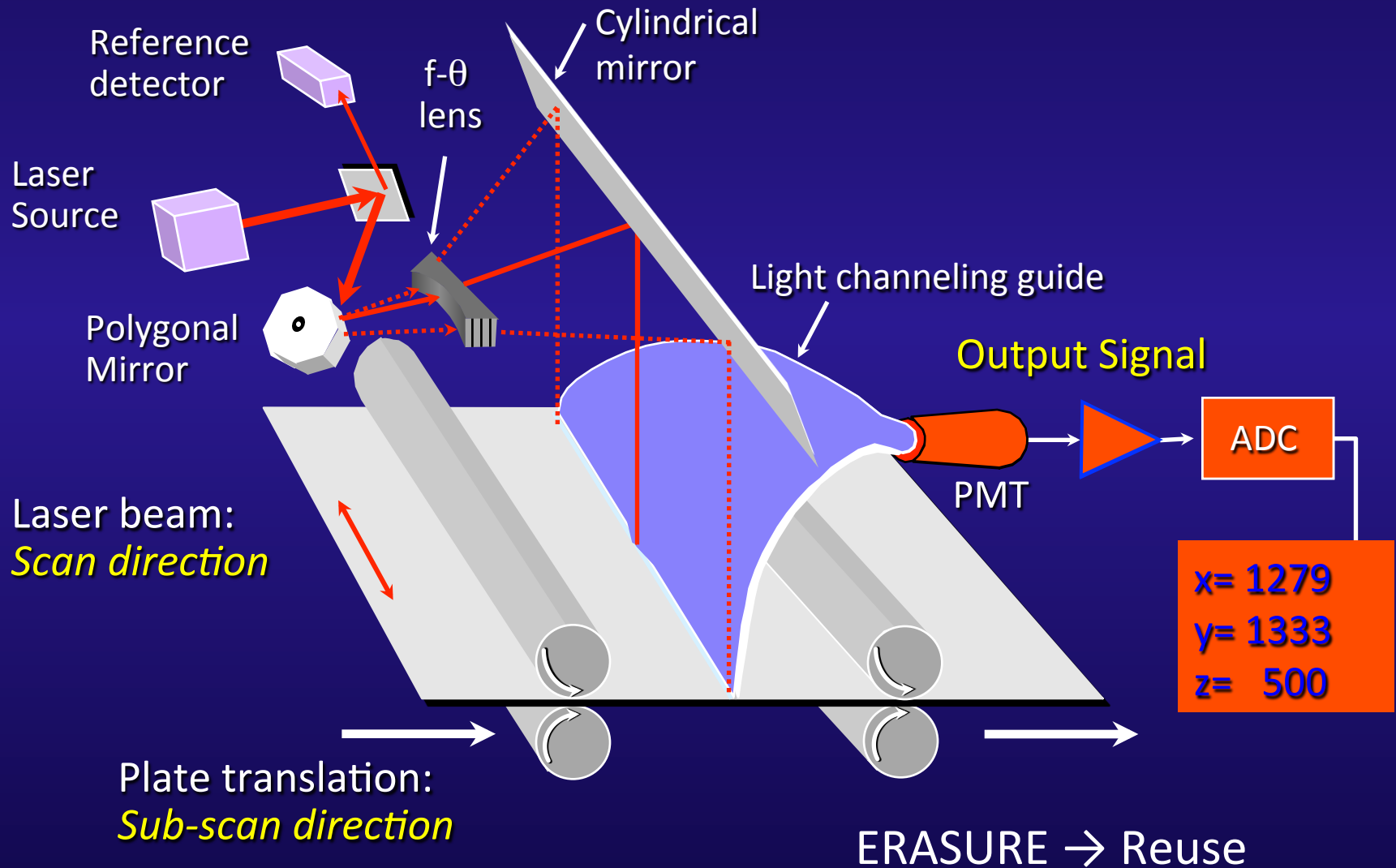
Various capabilities, sizes, throughput

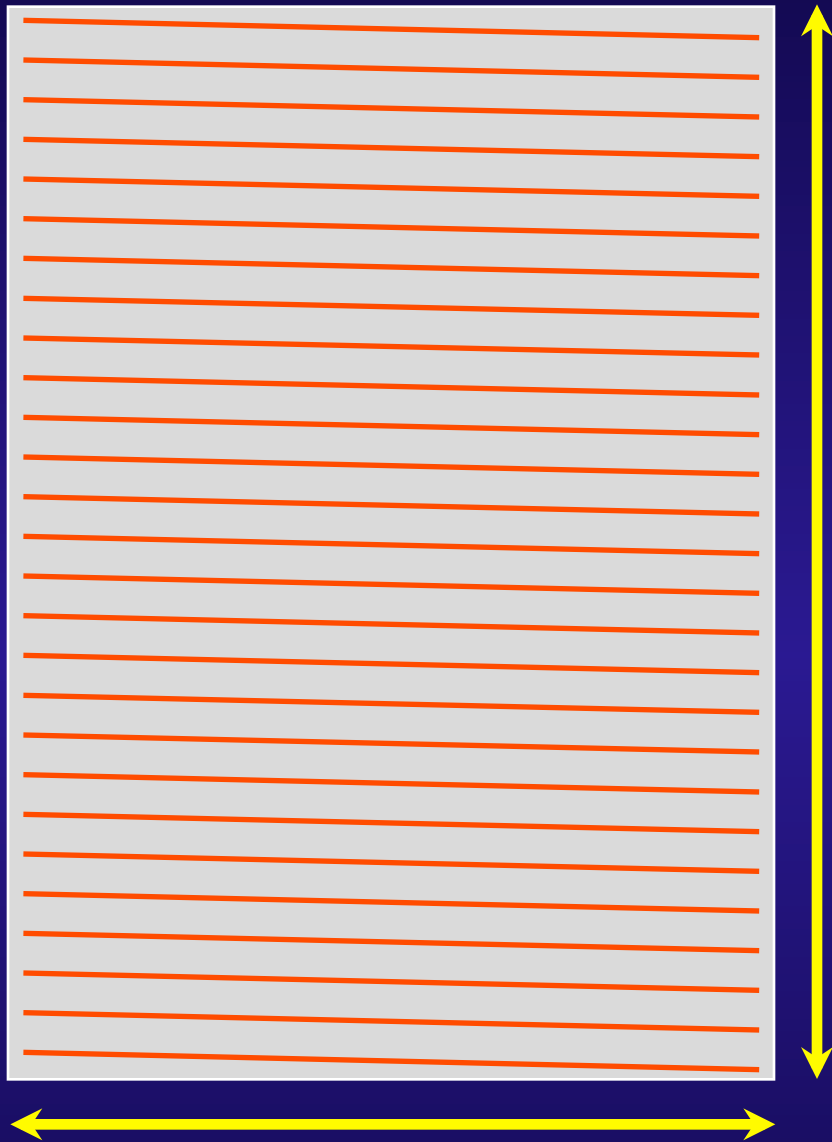


Photostimulated Luminescence



CR Point-scan readout





Sub-scan Direction
Plate translation

Typical CR resolution:

35 x 43 cm -- 2.5 lp/mm (200 μ m)

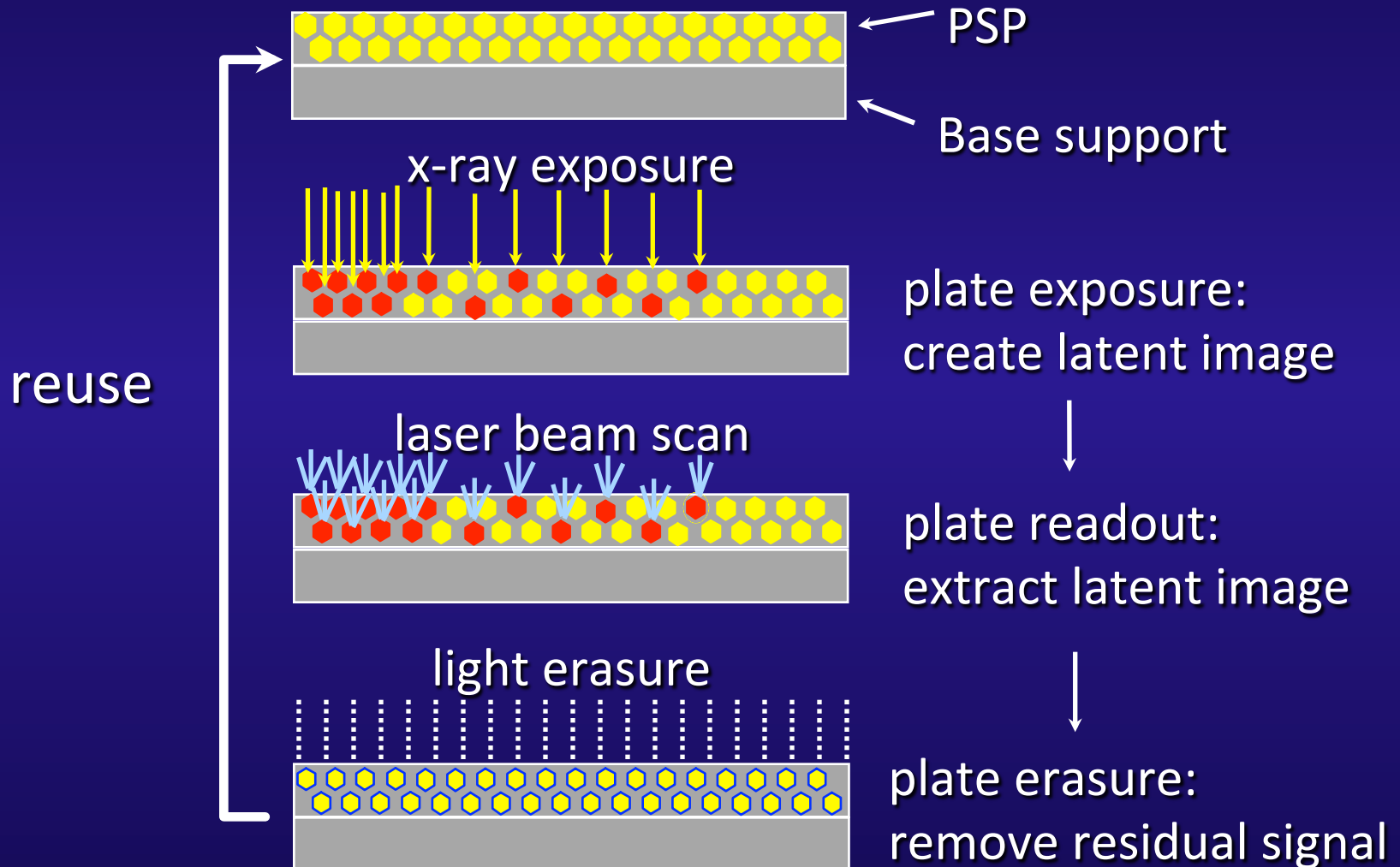
24 x 30 cm -- 3.3 lp/mm (150 μ m)

18 x 24 cm -- 5.0 lp/mm (100 μ m)

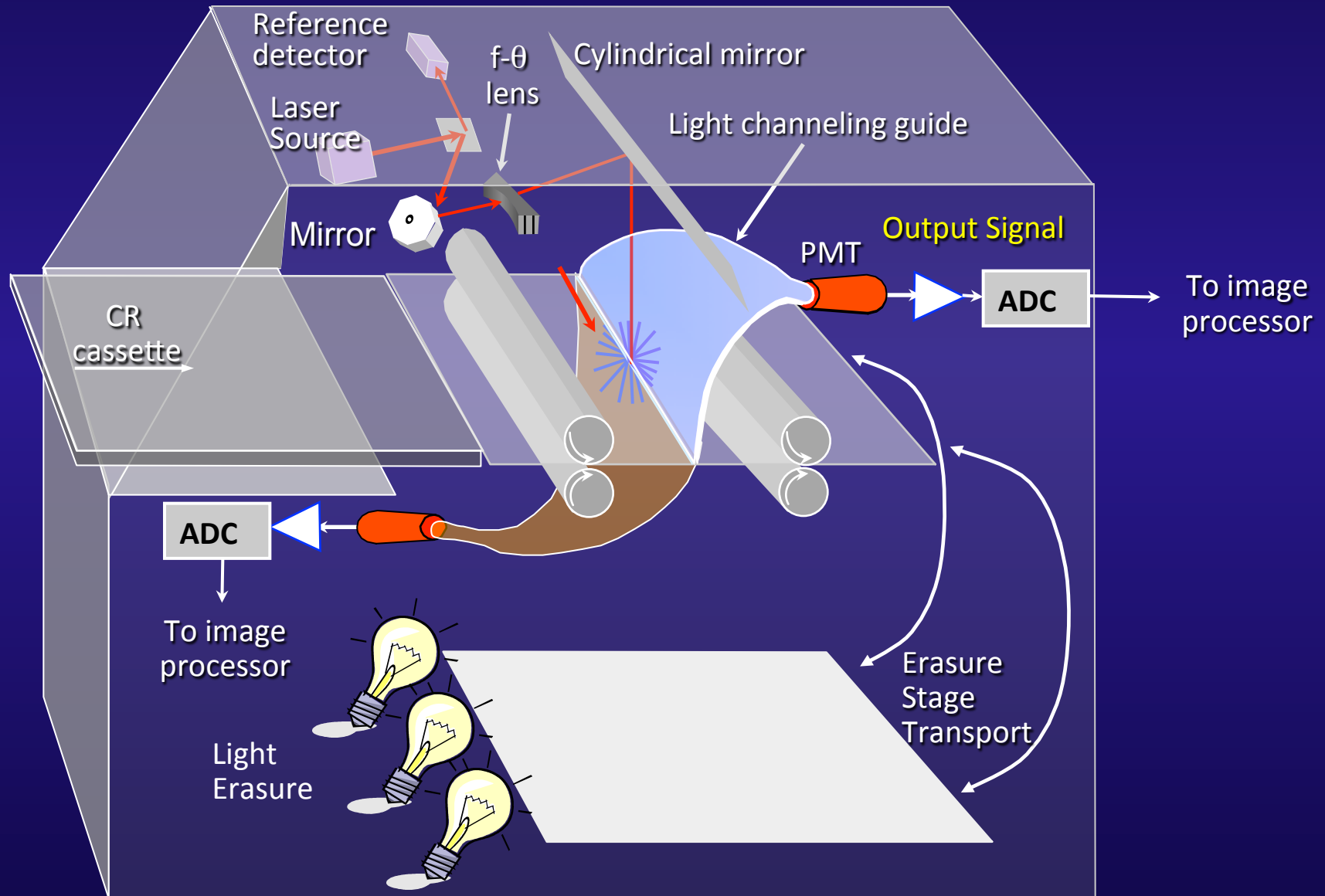
Screen/film resolution:
7-10 lp/mm (80 μ m - 25 μ m)

Scan Direction
Laser beam deflection

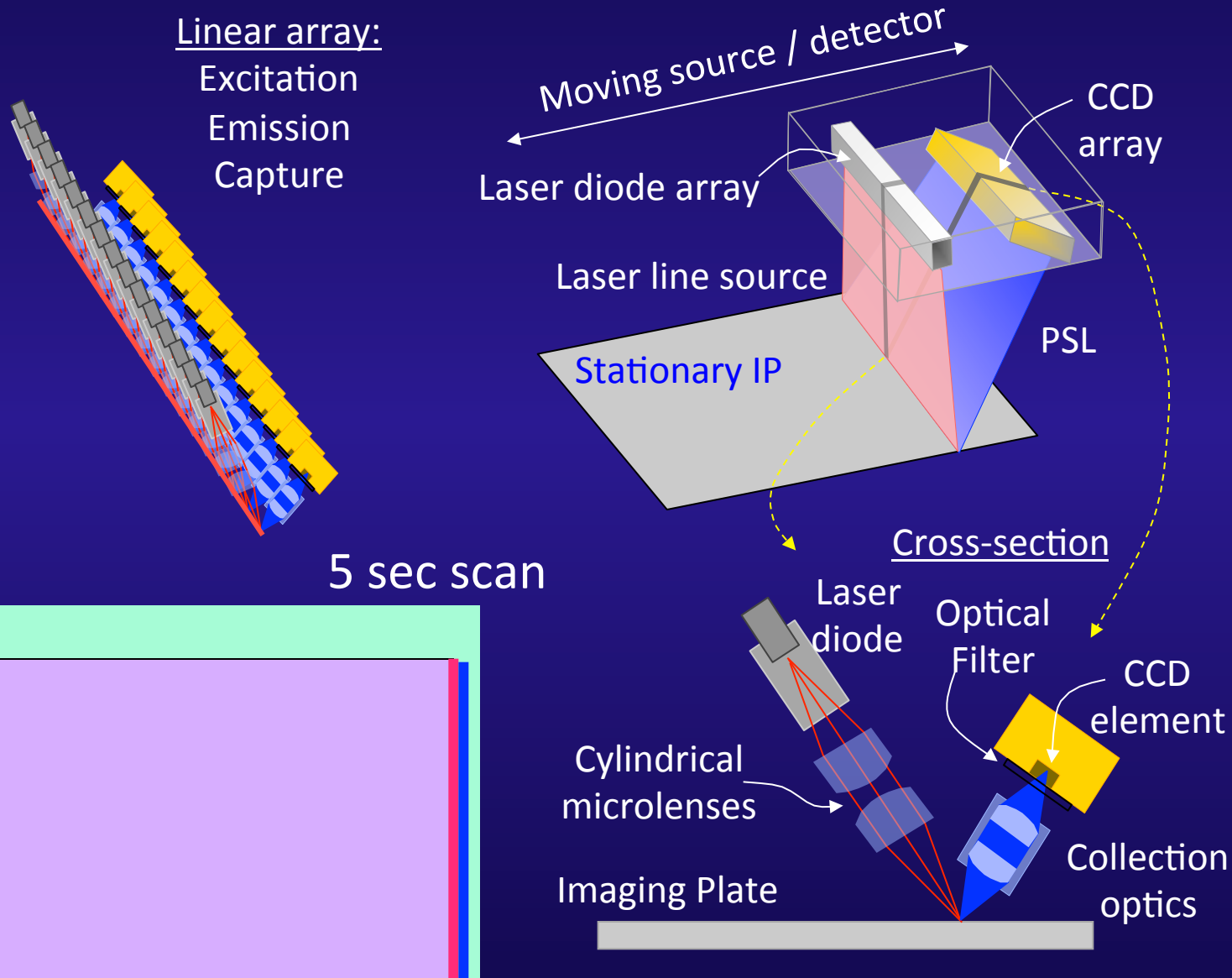
Phosphor Plate Cycle



Dual-side CR readout with transparent substrate



Parallel excitation *line-scan* PSP readout



“Direct” Radiography (DR)

....refers to the acquisition and capture of the x-ray image *without user intervention* (automatic electronic processing and display)

- “Indirect” detector: a conversion of x-rays into light by a scintillator, *and* light into electrons for signal capture
- “Direct” detector: a conversion of x-rays to electron-hole pairs with direct signal capture

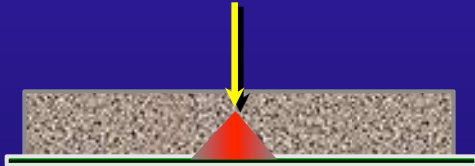
X-ray scintillator conversion

($\text{Gd}_2\text{O}_2\text{S}$, CsI compounds)

Unstructured (turbid) phosphor

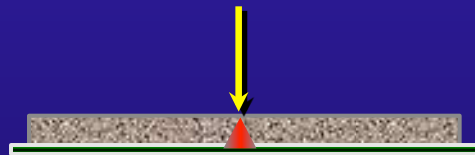
Thick Screen:

- Good Absorption
- Poor Resolution



Thin Screen:

- Poor Absorption
- Good Resolution



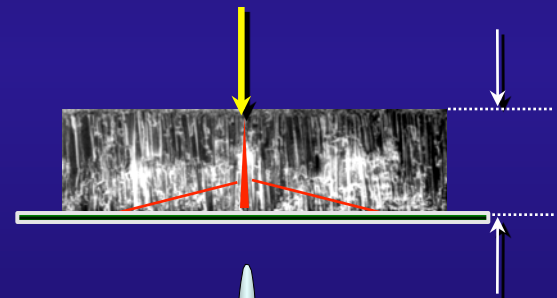
LSF

Resolution limit

Structured phosphor

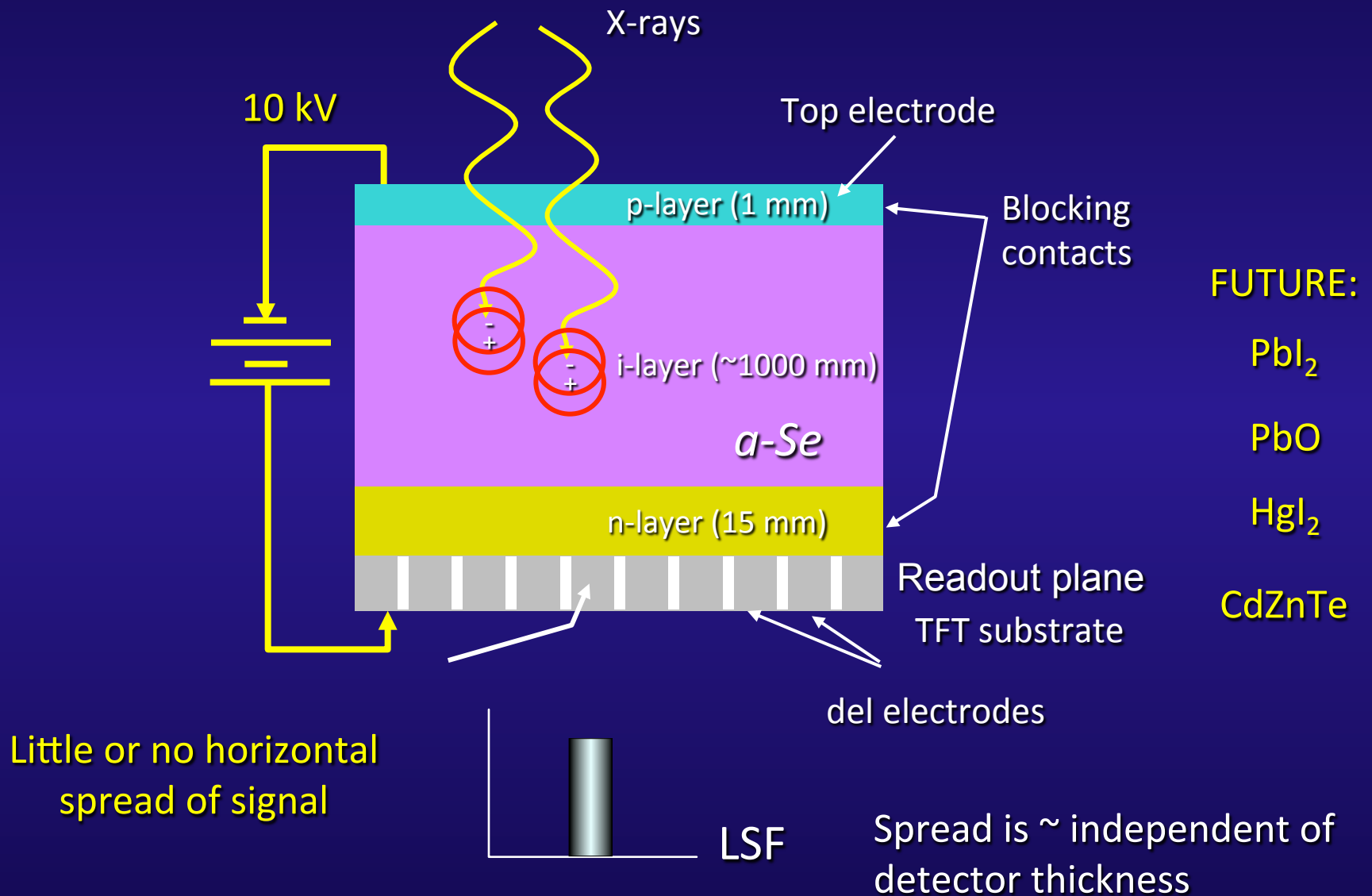
Thick Screen:

- Good Absorption
- Good Resolution



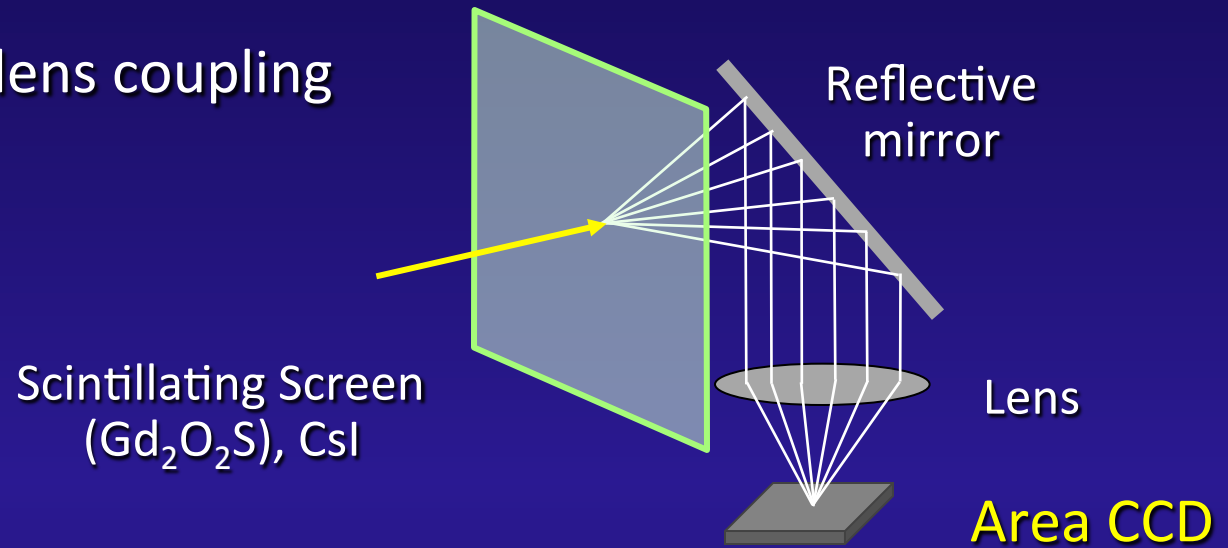
Light Pipe
(Optical Fiber)

Direct *semi-conductor* conversion

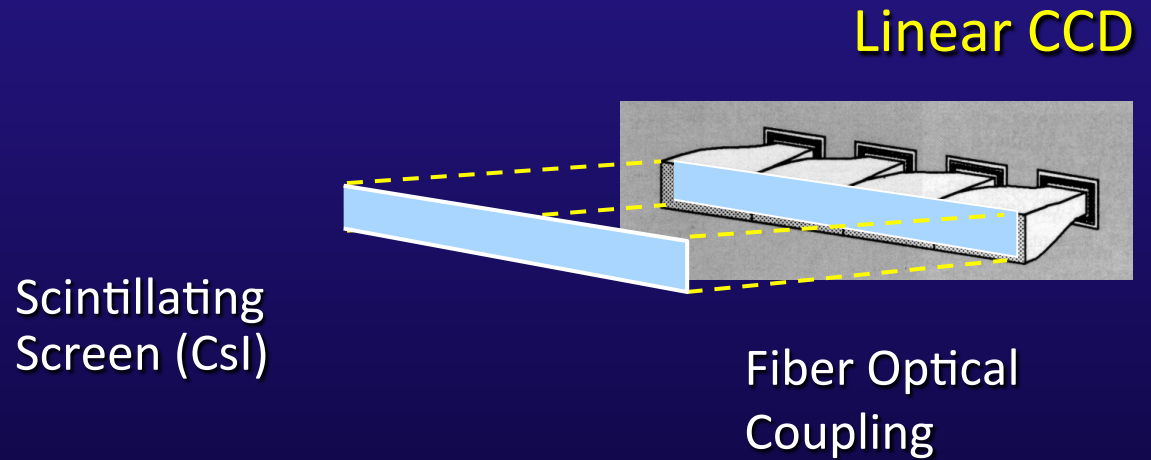


CCD-based DR systems

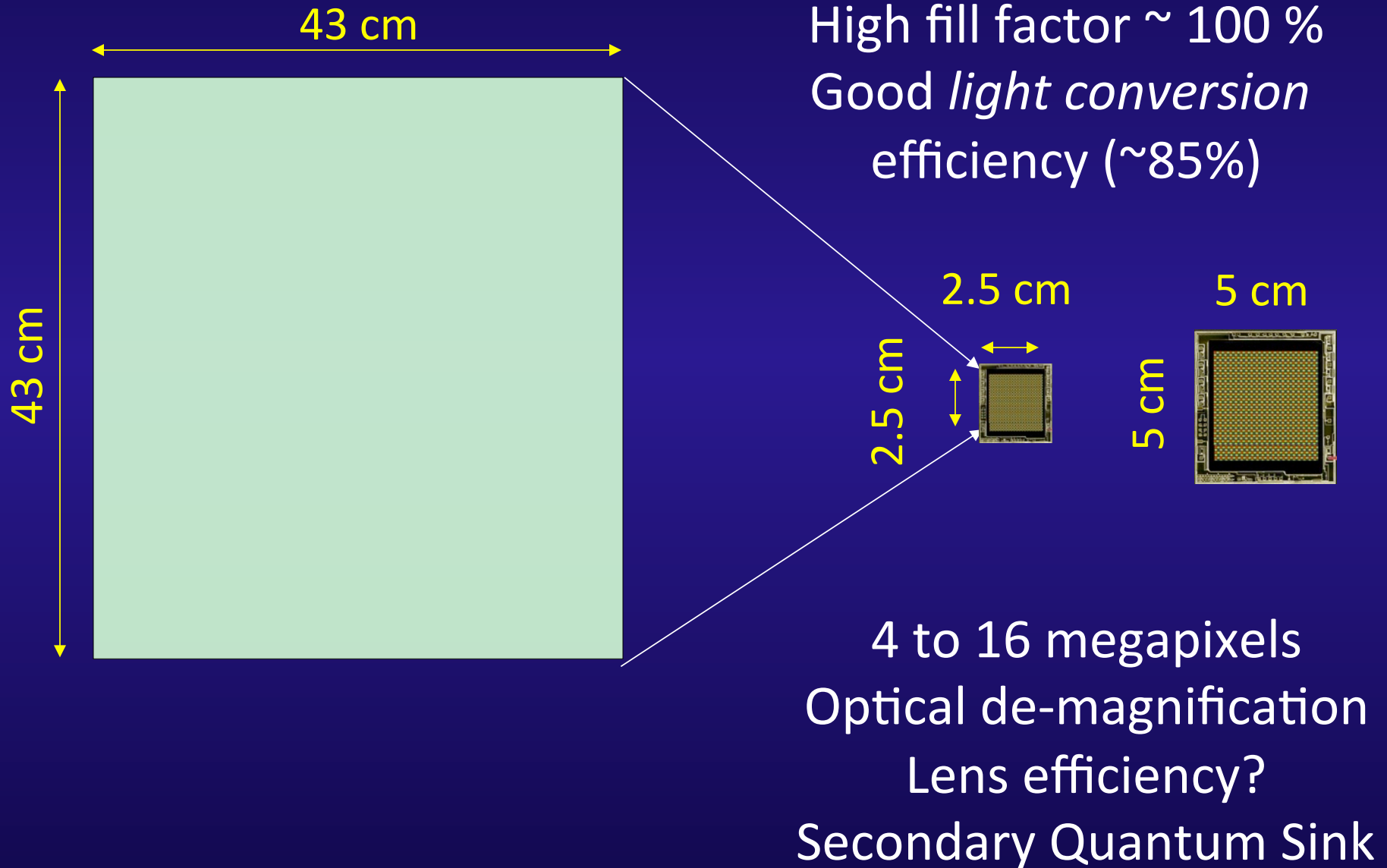
- Area Scintillator / lens coupling



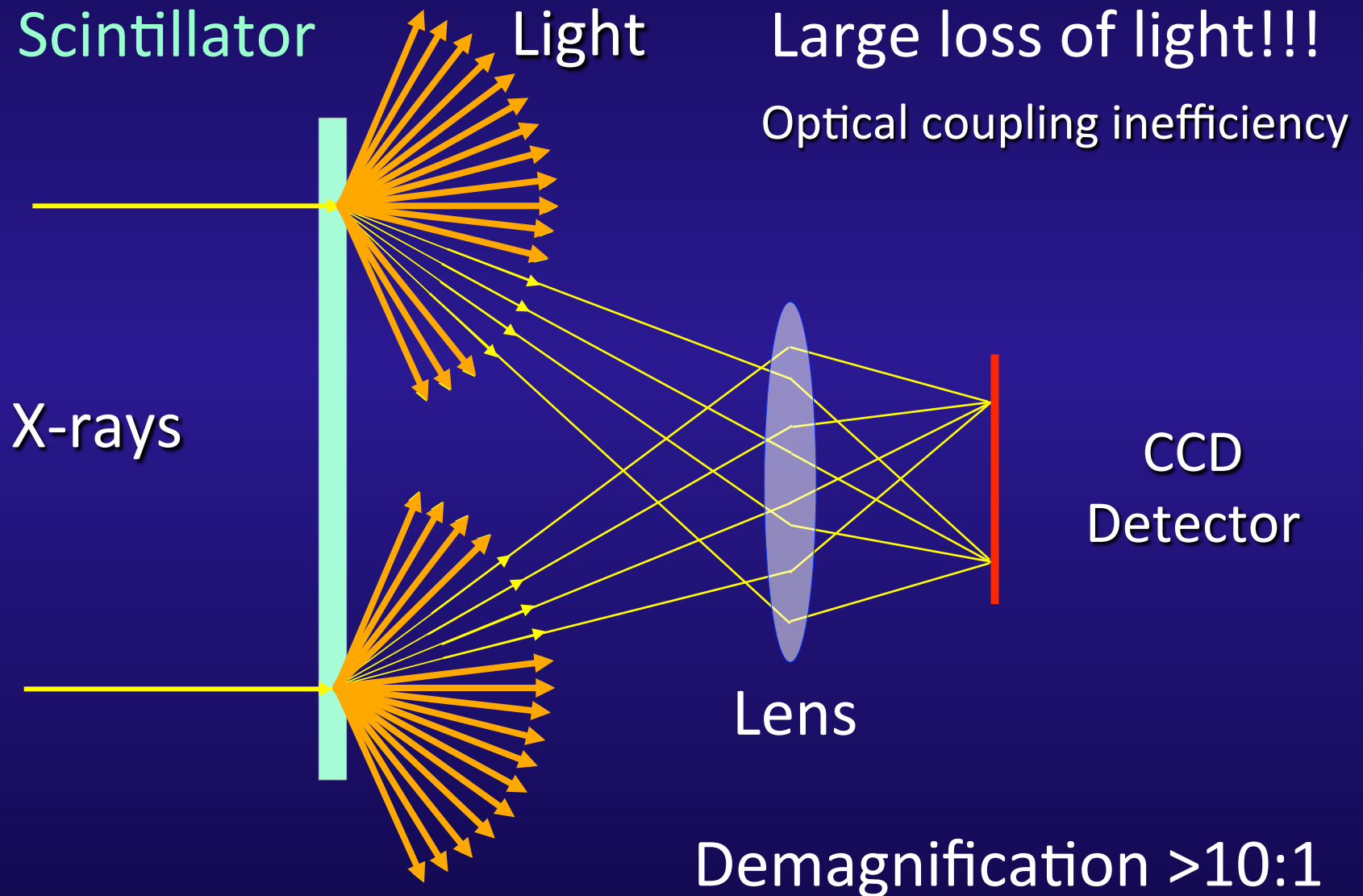
- Slot scintillator / fiberoptical coupling



CCD area detector



Light emission & Optical coupling



Optically coupled CCD systems

- Technology improvements have overcome quantum sink issues (lens / CsI phosphor)
- Relatively low cost (for integrated DR unit)
- Capable, OK image quality, higher dose

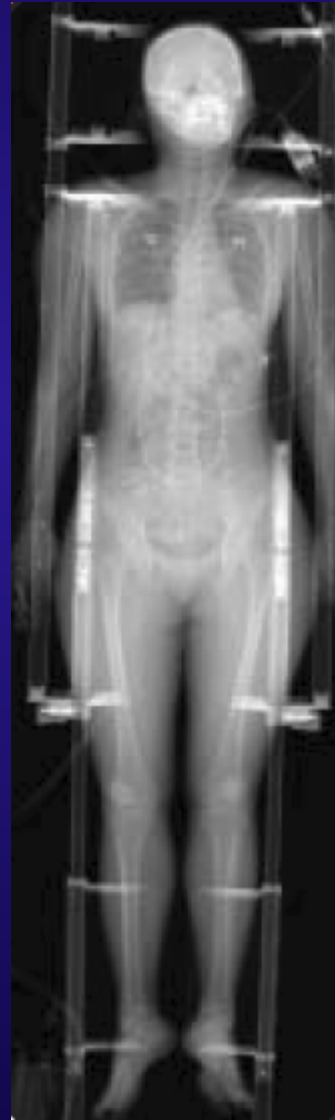


CCD slot-scan imaging

- “One dimensional” scanning acquisition
- Efficient scatter rejection
- Best dose efficiency
- Time-Delay-Integrate (TDI mode)
- “Effective DQE” in absence of scatter is comparable to CsI area detectors

Slot Scan CCD systems

No grid; Reduced scatter; Low dose



Trauma

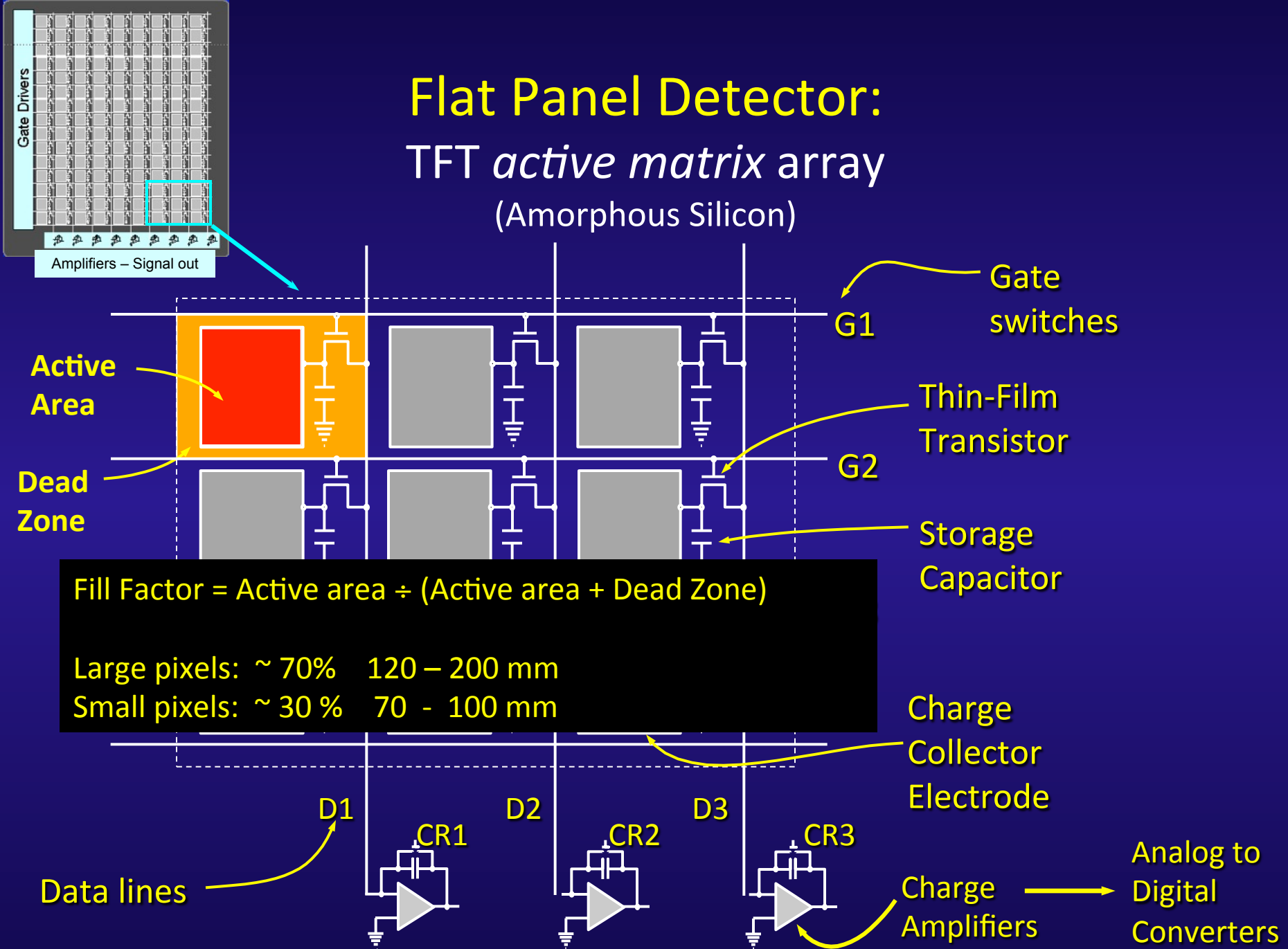


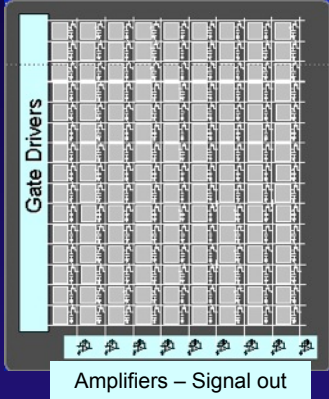
???

- Exposure time
- Patient motion
- Tube loading
- DQE



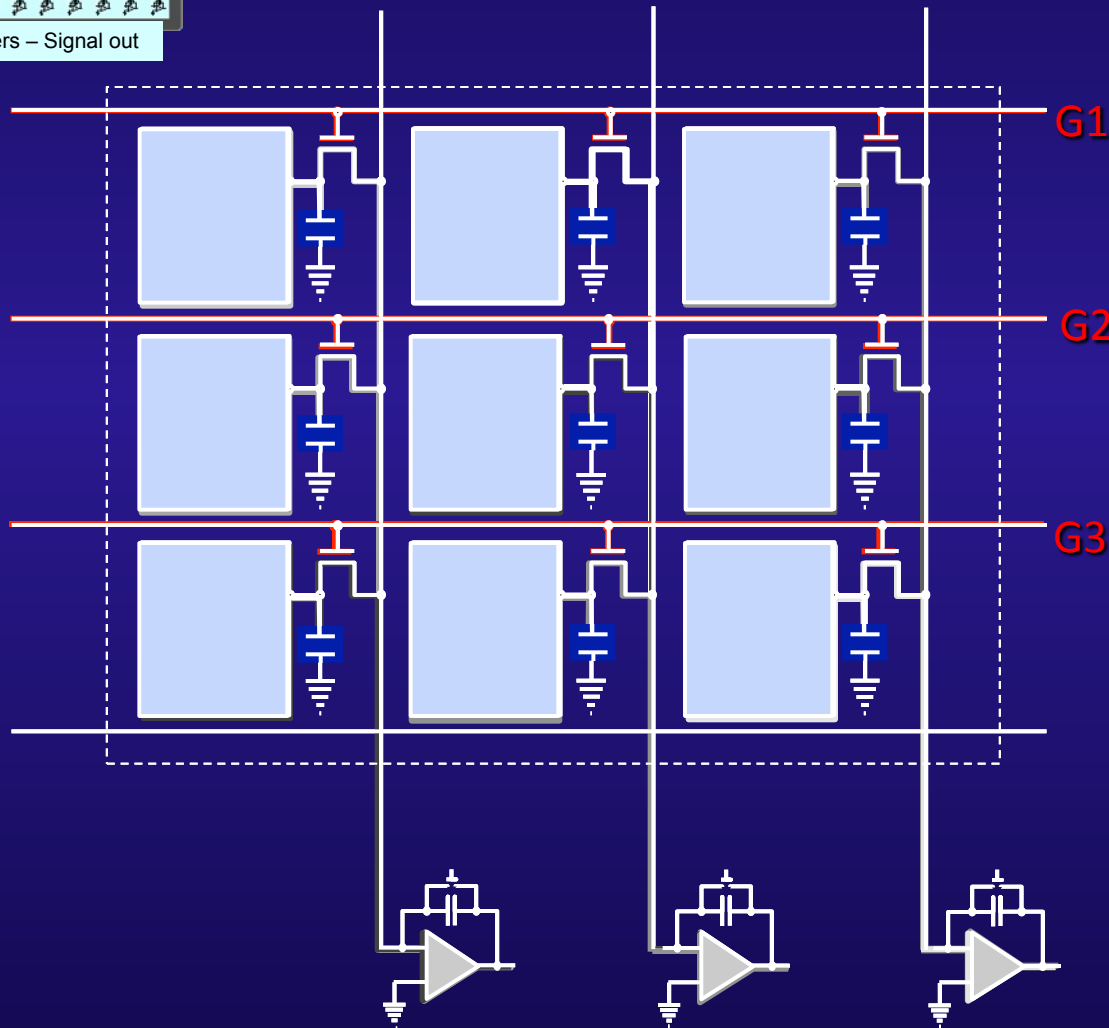
Flat Panel Detector: TFT *active matrix* array (Amorphous Silicon)





TFT *active matrix* array

Functional Illustration



Expose to x-rays

Store the charge

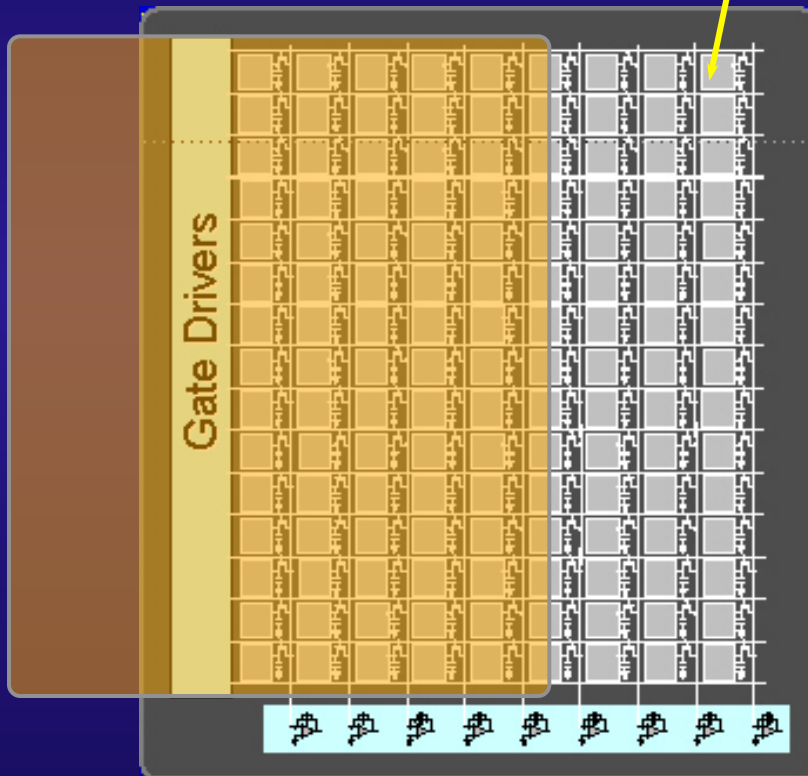
Active Readout
 Activate gates
 Amplify charge
 Convert to Digital

X-ray Indirect Detection

CsI phosphor / a-Si TFT

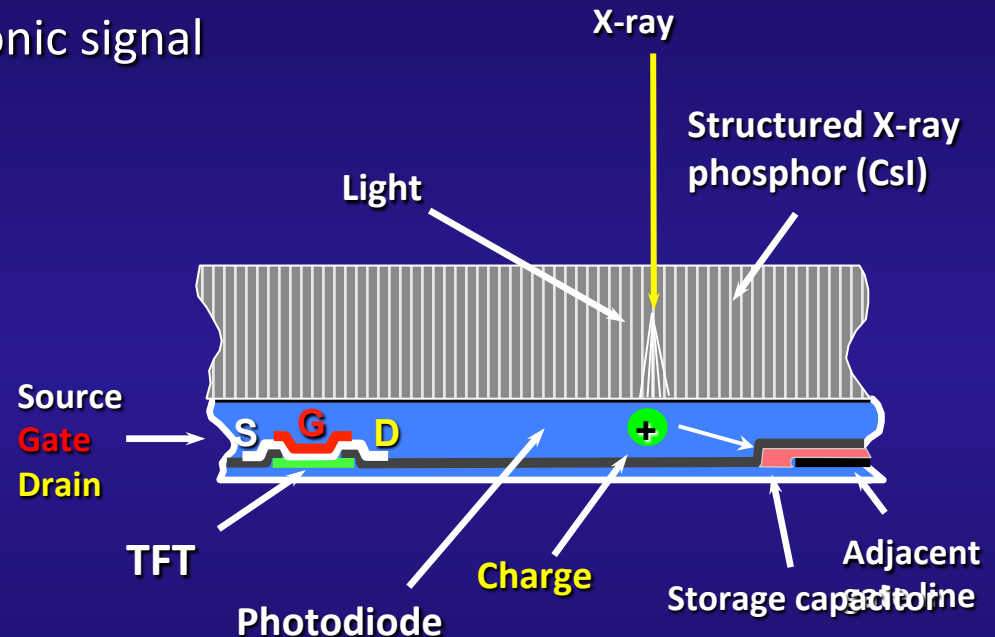
Scintillator:
X-rays to light

Photodiode:
Light to electronic signal



Amplifiers – Signal out

TFT array: Storage and readout

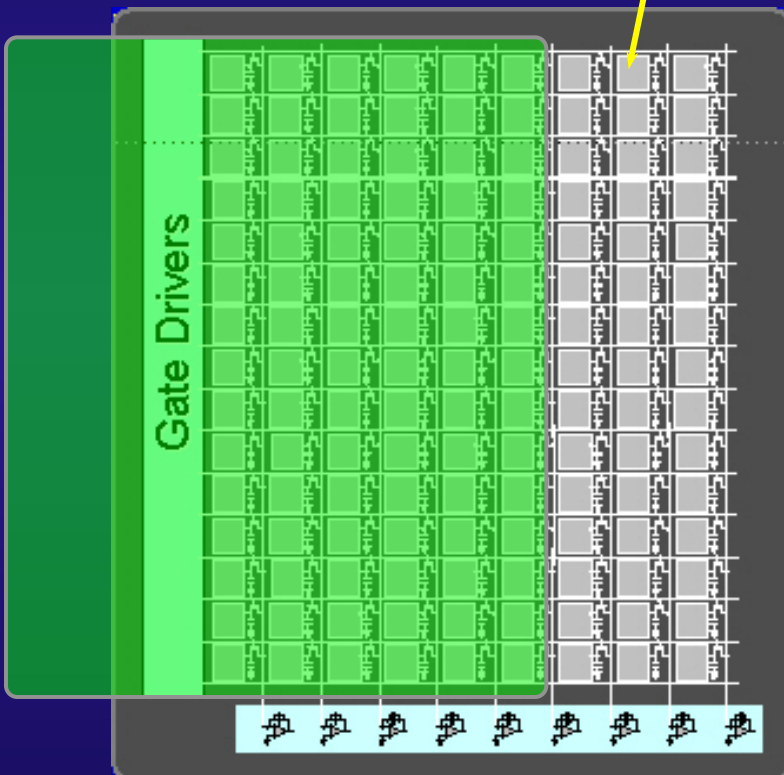


X-ray Direct Detection

a-Se layer / a-Si TFT array

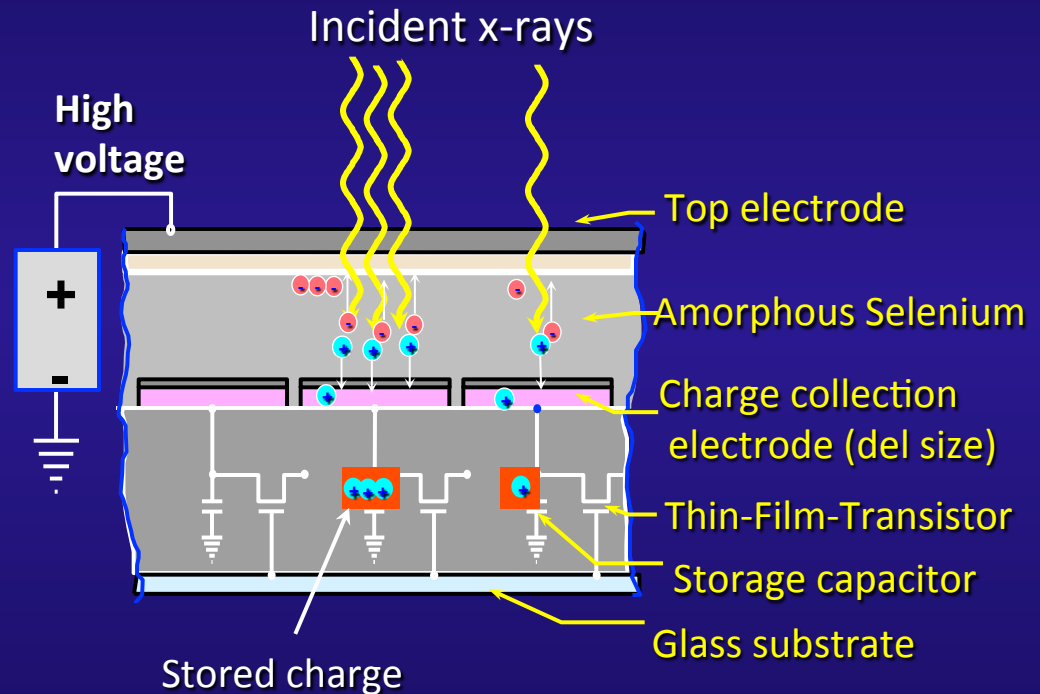
Semiconductor:
X-rays to charge

Charge collection
electrode



Amplifiers – Signal out

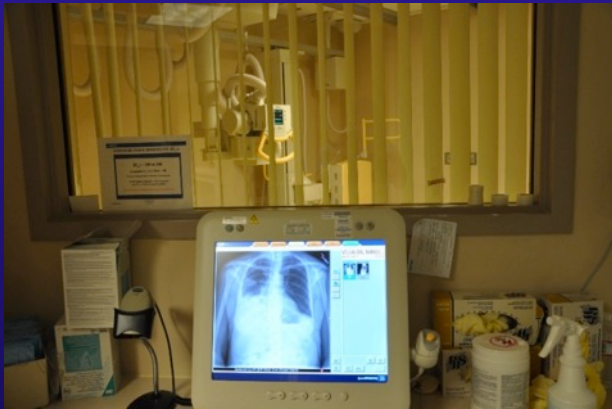
TFT array: Storage and readout



Alternate materials: PbI_2 , Hg_2

DR flat panel systems

Indirect



Direct

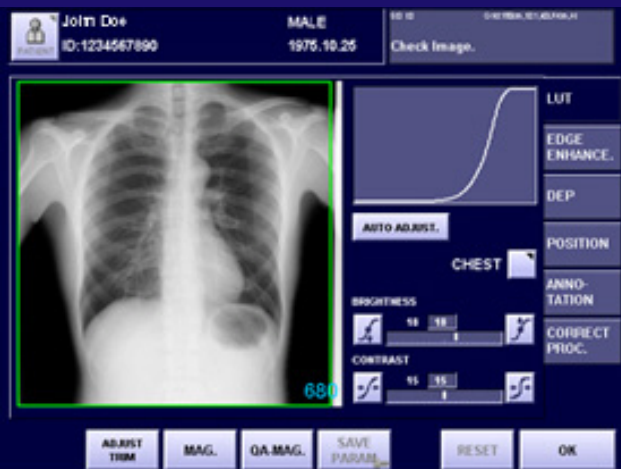


Flat panel portability

- Initial products introduced by Canon
 - Tethered, thick profile
- Wireless products now on the market
 - Trixell, Carestream, Canon, Source one ...



CR and DR mobile radiography



Tethered cassette

CR reader / processor

Wireless DR cassette

- Integrated
- Battery powered
- On-board computer and processing



Point of service direct imaging

- 14x17inch cassette...



Point of service direct imaging

- Preview image in 2-3 s



Point of service direct imaging

- For Processing image.... 15 s
- QC
- Annotation
- Send

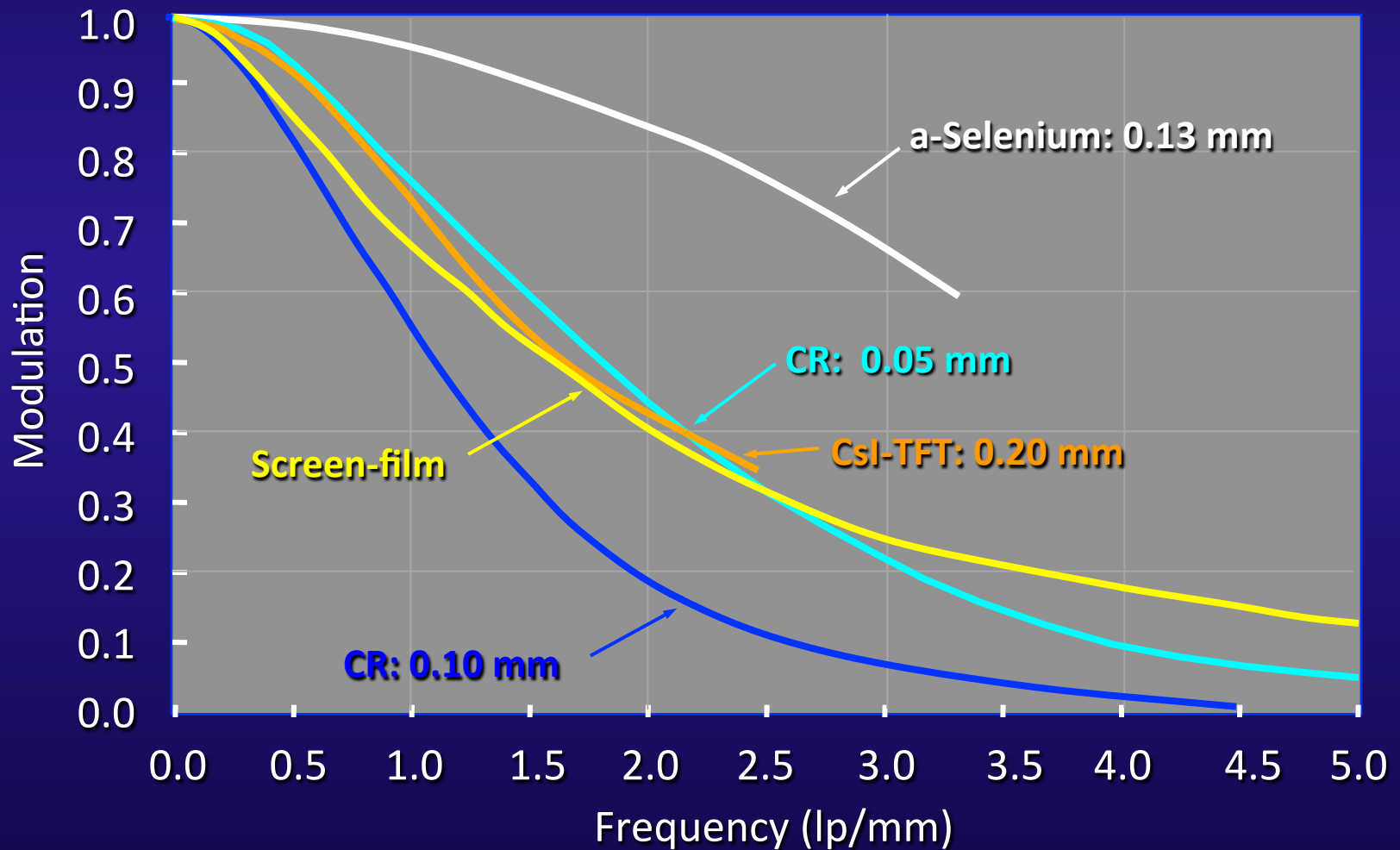


DR replacement trends

- Passive for active detector technology



Spatial Resolution – MTF

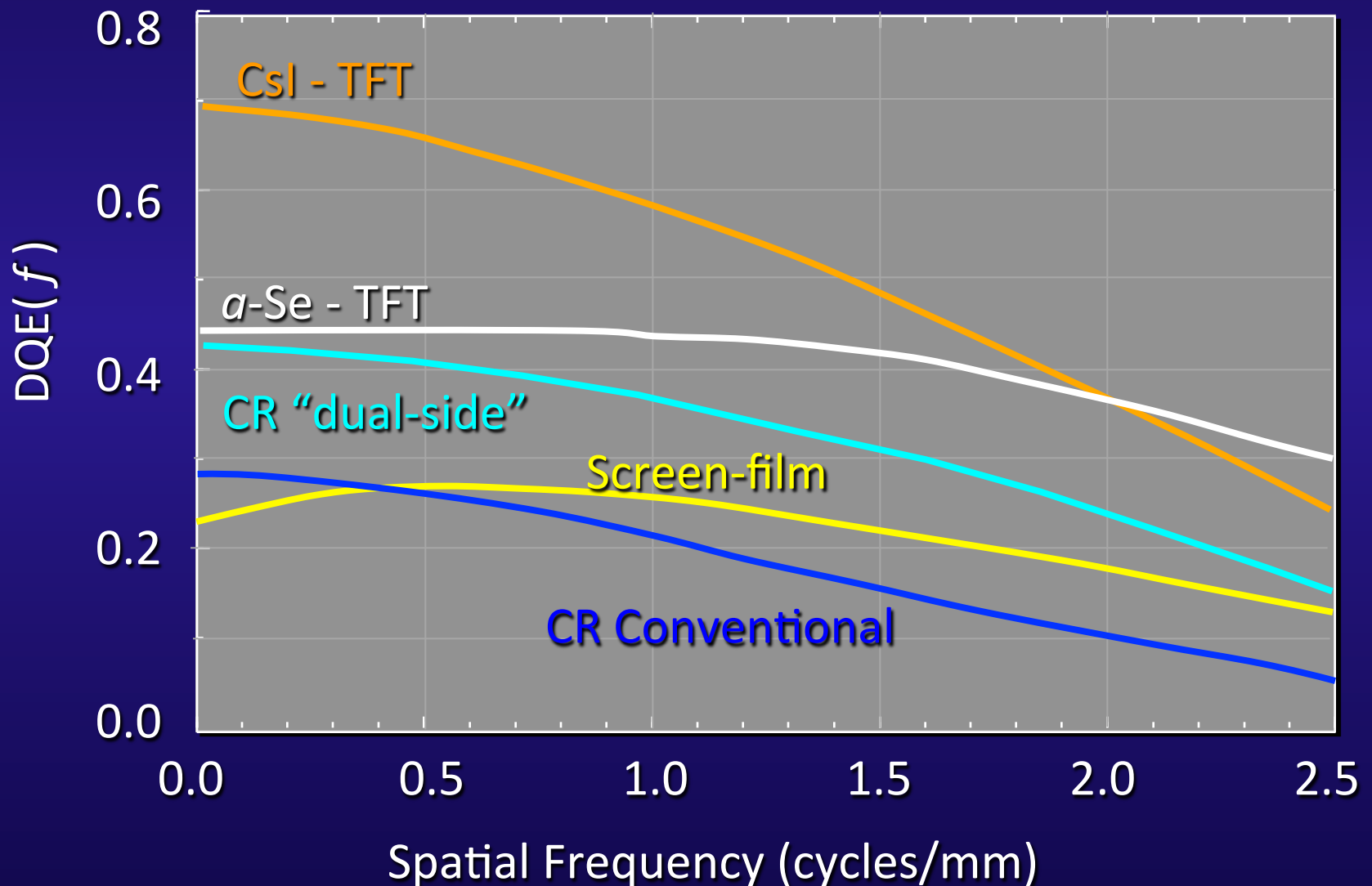


Detective Quantum Efficiency (DQE)

$$\text{DQE}(f) = \frac{\text{SNR}_{\text{out}}^2}{\text{SNR}_{\text{in}}^2} = \frac{\text{MTF}(f)^2}{\text{NPS}_{\text{N}}(f) \times q}$$

- A measure of the *information transfer efficiency* of a detector system
- Dependent on:
 - Absorption & conversion efficiency
 - Spatial resolution (MTF)
 - Conversion noise & electronic noise
 - Detector non-uniformities / pattern noise
 - **Not necessarily indicative of clinical performance**

Detective Quantum Efficiency Radiography



High DQE does not “guarantee” good image quality

- There is no substitute for appropriate radiographic technique
- Optimization of acquisition technique
 - kV, mAs, SID, filtration, anti-scatter grid
- For similar acquisition techniques and grid use, similar SNR requires dose proportional to DQE^{-1}
- “Effective DQE” concept takes into account clinical situations (magnification, grid)

Attribute	CR	DR	CCD
Positioning flexibility	****	**	**
Replacement for screen/film	****	**	**
DQE / dose efficiency	**	***	**
Patient throughput	*	***	**
X-ray system integration	**	*****	*****
Access to advanced technology applications	**	*****	***
Cost for comparable image throughput	***	**	***
Radiographer ease of use (manufacturer dependent)	*	***	**

SUMMARY

Enterprise distribution of images is crucial
for implementation and application of technology

- *Cassetteless, active detector* radiography devices are becoming the detectors of choice
- Proliferation of web-based PACS and unified patient database (instead of Radiology centric orientation) is coming
- New opportunities
 - Image acquisition and image processing tools
 - Imaging technology innovation for diagnosis and intervention